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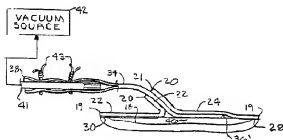
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(54) **SYSTEME ET METHODE DE RACCORDEMENT FLUIDIQUE**
(54) **FLUIDIC CONNECTION SYSTEM AND METHOD**

(57)

A wound dressing (10) includes a cover membrane (22) comprising a semi-permeable material with an adhesive-coated (30) skin contact surface (28). An opening (32) is formed in an interior portion of the membrane. An intermediate layer of material may be placed between the wound and the membrane contact surface for either absorbing fluids from the wound, e.g. with a hydrocolloid or hydrophilic material, or for passing such fluids to the opening with a synthetic material, e.g. rayon. A tube (34) includes a proximate end (36) fluidically communicating with the wound through the membrane opening. A distal end (38) of the tube is adapted for connection to a suction source (47) for draining the wound or a fluid source for introducing liquid medication to the wound. Both evacuation and introduction can be either active or passive. A wound treatment method is also disclosed.





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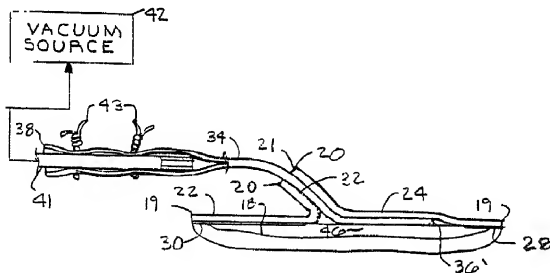
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(54) Title: FLUIDIC CONNECTION SYSTEM AND METHOD



(57) Abrégé/Abstract:

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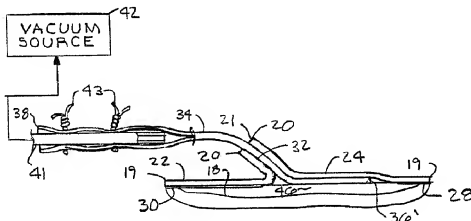
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(54) Title: FLUIDIC CONNECTION SYSTEM AND METHOD



(57) Abstract

A wound dressing (10) includes a cover membrane (22) comprising a semi-permeable material with an adhesive-coated (30) skin contact surface (28). An opening (32) is formed in an interior portion of the membrane. An intermediate layer of material may be placed between the wound and the membrane contact surface for either absorbing fluids from the wound, e.g. with a hydrocolloid or hydrophilic material, or for passing such fluids to the opening with a synthetic material, e.g. rayon. A tube (34) includes a proximate end (36) fluidically communicating with the wound through the membrane opening (32). A distal end (38) of the tube is adapted for connection to a suction source (47) for draining the wound or a fluid source for introducing liquid medication to the wound. Both evacuation and introduction can be either active or passive. A wound treatment method is also disclosed.

+ See back of page

FLUIDIC CONNECTION SYSTEM AND METHODBackground of the Invention1. Field of the Invention.

The present invention relates generally to fluidic
5 connection systems, and in particular to systems for draining
liquids from and introducing liquids to patients.

2. Description of the Relevant Art.

Various types of fluidic connection systems have
heretofore been devised to meet the requirements of particular
10 applications. In the medical field, fluidic connection systems
find many applications, including wound dressings and systems
for introducing fluids to and removing fluids from patients.

Wound dressings are typically applied over various
types of wounds to promote healing and to reduce the risk of
15 infection. Although various types of dressing materials have
been successfully employed, membranes comprising semi-permeable
materials are often preferred because they can increase patient
comfort and lower the risk of infection. Semi-permeable
membranes generally pass moisture vapors, but are generally
20 impervious to liquids. Thus, they can promote healing by
permitting a wound site to "breathe".

1 However, a problem can arise with semi-permeable
2 membranes when they are placed over draining wounds because
3 they tend to retain fluid. For example, surgical wounds
4 often tend to drain for a post-operative period of about
5 forty-eight hours. The fluid that can accumulate under such
6 a semi-permeable membrane during a draining period can
7 macerate the underlying tissue, cause infection and
8 otherwise inhibit healing. A procedure for alleviating this
9 problem involves periodically piercing the membrane,
10 draining the accumulated fluids and resealing the membrane
11 opening. However, such a procedure is time-consuming for
12 health care professionals and, unless it is conducted at
13 relatively frequent intervals, can be relatively ineffective
14 in dealing with the problems associated with trapped fluid
15 accumulation. Other procedures which involve opening or
16 changing wound dressings tend to have problems associated
17 with exposing a wound to a greater risk of infection and can
18 be uncomfortable for patients.

19 Another disadvantage with many previous wound dressings
20 is that they are not designed to accommodate the
21 introduction of various liquid medications, such as
22 antibiotics and growth factor solutions. The application of
23 growth factor solutions may be particularly important in the
24 regeneration of skin graft donor sites.

25 Catheters are another type of fluidic connection system
26 with medical applications. They are commonly used for
27 withdrawing fluids from or introducing fluids to patients'
28 bodies. For example, urethral catheters are inserted into
29 the bladder through the urethra for withdrawing urine.
30 Typical applications for urethral catheters include patients

1 who are incontinent or have otherwise lost voluntary control
2 of their bladder functions, e.g. a paraplegic with a spastic
3 bladder condition. However, patients fitted with urethral
4 catheters are often subjected to risks of bladder and
5 urinary tract infections.

6 To avoid some of these infection risks, condom
7 catheters have been devised which typically include a body
8 for placement over the penis and a bellows-type distal end
9 for resisting kinks and for connection to a drain tube.
10 However, condom catheters are susceptible to slippage and
11 can be difficult to maintain in place unless they are taped
12 to the patient's penis. Furthermore, there can be
13 difficulties in effectively draining sudden surges of urine,
14 which often back up and cause leakage problems.

15 Heretofore there has not been available a fluidic
16 connection system and method with the advantages and
17 features of the present invention.

18

19 Summary of the Invention

20

21 In the practice of the present invention, a fluidic
22 connection system is provided which includes a semi-
23 permeable membrane including a pair of panels each having a
24 perimeter and an edge strip. The membrane is formed by
25 connecting the panel edge strips together to form a seam
26 extending transversely across the membrane. The panels and
27 the membrane include inner and outer surfaces. A tube
28 opening extends through the seam between the panel edge

29

30

1 strips and between the membrane inner and outer surfaces.
2 The membrane inner surface is coated with an adhesive for
3 attachment to the skin of a patient.

4 A tube or sheath includes a proximate end extending
5 through the tube opening and a distal end positioned in
6 spaced relation from the membrane outer surface. In one
7 embodiment, the tube proximate end includes a side opening
8 which is positioned in proximity to the membrane inner
9 surface. In another embodiment the tube proximate end is
10 bifurcated by a pair of longitudinally-extending slits
11 separating a pair of tabs. A passage extends through the
12 sheath between its ends.

13 An inner conduit can be placed in the sheath passage
14 and can include a connection seal assembly for forming a
15 fluid-tight seal with the sheath. The inner, tubular
16 conduit can be provided with a funneled proximate end for
17 using the system as a condom catheter.

18 When the fluidic connection system is used as a wound
19 dressing, an intermediate layer of material can be applied
20 between the wound and the cover membrane inner surface.
21 Furthermore, the fluidic connection system of the present
22 invention can be used to secure a percutaneous drainage tube
23 within a patient, e.g. by inserting the percutaneous tube
24 through the sheath passage.

25 In the practice of the method of the present invention,
26 an intermediate layer of material can be applied to a wound
27 site and the cover membrane can then be placed thereover.
28 The cover membrane can be releasably, adhesively fastened to
29 the skin around a periphery thereof. A tube fluidically
30 communicates with the wound through an opening in the

5

1 membrane. Fluids from a draining wound can be evacuated
2 through the tube and liquid medication and irrigation can be
3 introduced through the tube to the wound site. The fluid
4 evacuation and introduction steps of the method can each be
5 accomplished both actively and passively, and can be
6 alternated in a wound treatment procedure. Additional steps
7 that can be included in the method of the present invention
8 include extending an inner conduit through the sheath and
9 sealing the inner conduit and the sheath together in a
10 fluid-tight engagement.

11

12 Objects and Advantages of the Preferred Embodiments

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14 The principle objects and advantages of the present
15 invention include: to provide a wound dressing; to provide
16 such a dressing which promotes the evacuation of drainage
17 fluids; to provide such a dressing which permits the
18 introduction of liquid medications; to provide such a
19 dressing which includes a semi-permeable membrane for
20 releaseable, adhesive attachment to the skin surface
21 surrounding a wound; to provide such a dressing which
22 protects against infection; to provide such a dressing which
23 promotes healing; to provide such a dressing which is
24 economical to manufacture, efficient in operation, capable
25 of a long operating life and particularly well adapted for
26 the proposed usage thereof; to provide a wound treatment
27 method; to provide a fluidic connection system and method;
28 to provide such a connection system and method which are
29 adaptable to various applications; to provide such a
30 connection system and method which can be utilized as a

1 condom catheter; to provide such a connection system and
2 method which are suitable for securing percutaneous tubing;
3 to provide such a connection system which infrequently
4 requires changing; and to provide such a connection system
5 and method which promote patient comfort, reduce risk of
6 infection, are usable with catheters of various
7 configurations and which are easy to apply and use.

8 Other objects and advantages of this invention will
9 become apparent from the following description taken in
10 conjunction with the accompanying drawings wherein are set
11 forth, by way of illustration and example, certain
12 embodiments of this invention.

13 The drawings constitute a part of this specification
14 and include exemplary embodiments of the present invention
15 and illustrate various objects and features thereof.

16

17 Brief Description of the Drawings

18

19 Fig. 1 is a top perspective view of a wound dressing
20 embodying the present invention.

21 Fig. 2 is an enlarged, vertical, cross-sectional view
22 of the dressing taken generally along line 2-2 in Fig. 1.

23 Fig. 3 is a top plan view of the dressing.

24 Fig. 4 is an enlarged, fragmentary, bottom perspective
25 view of the dressing, particularly showing a proximate end
26 of the tube.

27 Fig. 5 is an enlarged, fragmentary, top perspective
28 view of the dressing, particularly showing a tube closure
29 clip.

30

1 Fig. 6 is an enlarged, fragmentary, vertical, cross-
2 sectional view of the dressing, particularly showing the
3 tube connected to a vacuum source.

4 Fig. 7 is an enlarged, fragmentary, vertical, cross-
5 sectional view of the dressing, particularly showing a
6 resealable injection port mounted on a distal end of the
7 tube.

8 Fig. 8 is a top perspective view of a wound dressing
9 comprising a first modified embodiment of the present
10 invention.

11 Fig. 9 is a top plan view of a wound dressing
12 comprising a second modified embodiment of the present
13 invention with an intermediate material layer between the
14 wound site and a cover membrane.

15 Fig. 10 is an enlarged, fragmentary, vertical, cross-
16 sectional view of the second modified wound dressing
17 embodiment, taken generally along line 10-10 in Fig. 9.

18 Fig. 11 is a perspective view of a fluidic connection
19 system comprising a third modified embodiment of the present
20 invention, shown in combination with a drain conduit and
21 fluid connection vessel for use as a condom catheter and
22 urine collection system.

23 Fig. 12 is a top plan view of the connection system
24 being applied as a condom catheter.

25 Fig. 13 is an enlarged, vertical, cross-sectional view
26 of the connection system taken generally along line 13-13 in
27 Fig. 12.

28 Fig. 14 is an enlarged, fragmentary, vertical, cross-
29 sectional view of the connection system, particularly
30 showing a funnel end of an inner conduit.

8

1 Fig. 15 is a top plan view of the connection system.

2 Fig. 16 is a side elevational view of the connection
3 system.

4

5 Detailed Description of the Preferred Embodiments

6

7 I. Introduction and Environment

8

9 As required, detailed embodiments of the present
10 invention are disclosed herein; however, it is to be
11 understood that the disclosed embodiments are merely
12 exemplary of the invention, which may be embodied in various
13 forms. Therefore, specific structural and functional
14 details disclosed herein are not to be interpreted as
15 limiting, but merely as a basis for the claims and as a
16 representative basis for teaching one skilled in the art to
17 variously employ the present invention in virtually any
18 appropriately detailed structure.

19 Certain terminology will be used in the following
20 description for convenience and reference only and will not
21 be limiting. For example, the words "upwardly",
22 "downwardly", "rightwardly" and "leftwardly" will refer to
23 directions in the drawings to which reference is made. The
24 words "inwardly" and "outwardly" will refer to directions
25 toward and away from, respectively, the geometric center of
26 the structure being referred to. Said terminology will
27 include the words specifically mentioned, derivatives
28 thereof and words of similar import.

29

30

1 Referring to the drawings in more detail, the reference
2 numeral 10 generally designates a wound dressing embodying
3 the present invention. The dressing 10 is adapted for
4 protecting and treating a variety of wounds, such as that
5 shown at 12. Without limitation on the generality of the
6 useful applications of the present invention, the dressing
7 10 may be applied over burns, cuts, scrapes and ulcers of
8 various types, e.g. diabetic, decubitus, peripheral
9 vascular disease, venous stasis and trauma ulcers.

10 Skin ulcers are a common problem among many diabetics,
11 and are often brought on by poor blood circulation and nerve
12 damage associated with diabetes. The treatment of such
13 ulcers often involves grafting skin from a relatively
14 healthy donor site to an ulcerous wound site. Split
15 thickness surgical skin graft techniques may be employed to
16 obtain skin grafts from donor sites that can then heal
17 spontaneously. Full thickness skin grafts, on the other
18 hand, generally require closure of the donor site. It will
19 be appreciated from the following description that the wound
20 dressing and treatment method of the present invention is
21 particularly well adapted for the protection and
22 regeneration of skin graft donor sites by providing a single
23 dressing which facilitates both fluid drainage and growth
24 factor introduction.

25 The wound site 12 is surrounded by healthy skin 16. A
26 fibrin layer 18 forms at the wound site 12 from fibrinogen
27 by the action of thrombin and the clotting of blood (Figs.
28 2 and 6). Surgical wounds, including those associated with
29
30

skin grafts, normally drain fluid. The fluid drainage from a surgical wound is generally heaviest during a post-operative period of about forty-eight hours.

II. Wound Dressing 10

5 The wound dressing 10 generally comprises a cover membrane 22 with an interior portion 24 surrounded by a perimeter 26. The membrane 22 includes a skin contact surface 28 with an adhesive coating 30. The membrane 22 preferably comprises a breathable semi-permeable material characterized by
10 an ability to pass moisture vapors and an imperviousness to liquids. The adhesive coating 30 should likewise be semi-permeable. Such membrane materials are commercially available, an example being material referred to as "Tagoderm"*, which is available from the 3M (Minnesota Mining and Manufacturing)
15 Company of St. Paul, Minnesota. Other semi-permeable materials are available and can be successfully employed with the present invention. A protective backing 23 is placed over the adhesive coating 30 on the membrane skin contact surface 28 until the membrane 22 is ready for application.

20 The membrane 22 comprises a pair of panels 19 with inner, upturned edges 20 which can be adhesively joined together to form a seam 21 which extends transversely across the membrane 22 and projects generally upwardly therefrom. The panels 19 can be secured together at the seam 21 by the
25 adhesive coating 30 to form the seam 21.

A tube or sheath 34 includes a proximate end 36 located under the membrane 22 and a distal or free end 38. The tube 34 can be inserted through the seam 21 which forms an

* Trade-mark

opening 32 between the panel edge strips 20 at approximately the centre of the membrane 22. A relatively short length of the tube 34 adjacent to its proximate end 36 is shown under the membrane 22, but greater lengths of the tube 34 could be placed
5 under the membrane 22. As shown in Fig. 4, the tube proximate end 36 is open, and adjacent to the proximate end 36 an opening is formed. Preferably the tube opening 39 projects downwardly, i.e. away from the membrane skin contact surface 28. The short length of the tube 34 which is located under the membrane 22
10 can be releaseably secured to the skin contact surface 28 by the adhesive coating 30, preferably with the tube opening 39 facing downwardly.

The tube 34 can comprise, for example, a flexible, plastic tube of the type that is commonly used as a protective
15 sheath for protection of sterility for percutaneous intravenous catheter placement. Such sheaths are commercially available from Aero International, Inc. of Reading, Pennsylvania.

At its distal end 38, the tube 34 is adapted for: 1) closure with a variety of suitable closure devices; 2)
20 connection to various active and passive fluid collection devices for draining and evacuating fluid from the wound site; and 3) connection to various fluid source devices for actively and passively introducing fluid to the wound site.

Fig. 5 shows a bifurcated clip 240 for releaseably
25 closing and sealing the distal end 238 of tube 134, which is folded upon itself as shown.

12

1 Fig. 6 shows a vacuum tube end 41 inserted in the tube
2 distal end 38 and secured therein by ties or ligatures 43.
3 The vacuum tube 41 fluidically communicates with a suction
4 or vacuum source 42 for actively draining fluid from the
5 wound site. The suction or vacuum source 42 may comprise a
6 relatively simple, hand-actuated bulb or bellows, or it may
7 comprise a more sophisticated motorized pump which can be
8 actuated at predetermined time intervals or in response to
9 wound site conditions such as an accumulation of fluid under
10 the membrane 22.

11 Fig. 7 shows an injection port 44 sealed to the tube
12 distal end 38 by a band 45. The injection port 44 includes
13 a sleeve 47 which can extend into the tube 34 to protect it
14 from needle puncture. The injection port 44 can be of the
15 type which is designed for reuse and which automatically
16 reseals after being punctured by a syringe needle. It will
17 be appreciated that a wide variety of devices can be
18 employed for connecting the tube distal end 38 to various
19 liquid medication sources.

20

21 III. Treatment Method

22

23 According to the treatment method of the present
24 invention, the protective backing 23 is removed from the
25 membrane contact surface 28 to expose the adhesive coating
26 30 and the membrane 22 is placed over a wound site 12 with
27 its contact surface 28 down. The membrane perimeter 26 is
28 pressed against the healthy skin 16 surrounding the wound
29 site 12 to preferably form a relatively liquid-tight
30 adhesive bond therebetween. Various adhesive preparations

13

1 are commercially available for supplementing the bonding
2 action of the adhesive coating 30 in bonding the membrane
3 contact surface 28 to the healthy skin 16. The membranes 22
4 may be provided in various sizes to accomodate wounds of
5 different sizes. A sufficiently large membrane 22 should
6 normally be selected to provide ample overlap of the
7 perimeter 26 over the healthy skin 16 to insure a good bond
8 therebetween.

9 The tube distal end opening 39 may be placed directly
10 over the approximate center of the wound site 12, or it may
11 be placed eccentrically or at a depending location with
12 respect to the wound site 12. A dependent or lower position
13 for the opening 39 with respect to the wound site 12 may be
14 preferred to facilitate fluid drainage. The dressing 10 may
15 be applied promptly after a wound is inflicted, e.g.
16 immediately after the graft removal procedure and a skin
17 graft operation. To reduce the risk of infection, it may be
18 advisable to promptly cover the open wound site 12. The
19 wound dressing 10 may be kept in a sterile package until it
20 is needed. Such sterile packages and packaging techniques
21 are well known. For example, ethylene oxide may be used to
22 sterilize the dressing 10 prior to placement in a suitable
23 sterile package. The protective backing 23 is removed from
24 the membrane 22, thereby exposing its adhesive-coated
25 contact surface 28.

26 With the membrane 22 thus secured, a chamber 46 is
27 formed between the wound site 12 and the membrane contact
28 surface 28, and is surround by the membrane perimeter 26.
29 The chamber 46 fluidically communicates with the membrane
30 opening 32. In an evacuation mode of operation, such as

1 might be desirable for forty-eight hours or so after removal
2 of a split-thickness skin graft at a donor site, fluid 20
3 which accumulates in the chamber 46 is communicated through
4 the opening 32 and thence through the tube 34 for collection
5 and disposal. In a passive evacuation mode of operation,
6 the fluid 20 is evacuated through capillary action, or by
7 gravity with the opening 32 at a dependent, lower location
8 in relation to the wound site 12. Such a capillary, passive
9 drainage action may be sufficient for draining the wound
10 site 12 in many situations. Alternatively, an active
11 evacuation mode of operation involves attaching the tube 34
12 to the suction/vacuum source 42 whereby the fluid 20 is
13 positively drawn from the wound site 12 and the chamber 46.
14 Such an active evacuation mode of operation may be preferred
15 when the dressing 10 is used in connection with a
16 hydrophilic colloidal material (hydrocolloid), as will be
17 explained in more detail hereinafter.

18 It may be desirable to operate the wound dressing 10 in
19 an introduction mode of operation whereby medications such
20 as antibiotics and growth factor solutions are introduced to
21 the wound site 12. In this mode of operation, the tube
22 distal end 38 is connected to a liquid solution source,
23 which may comprise a syringe or any of various liquid
24 containers for passive, gravity-induced introduction.
25 Various adaptors, valves and injection needle ports are
26 available for fluidically coupling the tube 34 to a wide
27 variety of liquid solution sources. For example, many such
28 connectors and adaptors are available from Aero
29
30

15

1 International, Inc. of Reading, Pennsylvania. Such
2 connecting devices are commonly used in connection with the
3 intravenous introduction of various liquid solutions.

4 In an active introduction mode of operation, solutions
5 may be pumped through the tube 34 into the chamber 46 for
6 application to the wound site 12.

7 The evacuation and introduction treatment steps can be
8 timed and sequenced as necessary to achieve the treatment
9 objectives. For example, treatment of a skin graft donor
10 site may involve fluid withdrawal and drainage for about two
11 days immediately following the skin graft operation,
12 followed by treatment steps comprising the introduction of
13 antibiotics and/or growth factor solutions to the wound
14 site. The evacuation and introduction steps can be
15 alternated, and the intervals between such steps can be
16 progressively increased or decreased as necessary to
17 facilitate healing. As the wound heals, progressively
18 smaller amounts of fluid will ooze therefrom and the
19 frequency and duration of the drainage operations can be
20 correspondingly reduced and finally discontinued altogether.

21 It will be appreciated that the wound dressing and
22 treatment method of the present invention are broadly
23 concerned with introducing fluid to wound sites and
24 evacuating fluid therefrom. The fluid introduction and
25 evacuation procedures described herein can be performed
26 indefinitely without having to change the dressing 10. The
27 tube 34 cooperates with the membrane 22 to permit the same
28 dressing 10 to be used for both procedures, which may be
29
30

1 alternated as often as necessary. Infection risks and
2 patient discomfort can be reduced by minimizing wound
3 dressing changes.

4 The removal of toxins and bacteria from wounds is an
5 important aspect of the fluid drainage phase of the healing
6 process. The wound dressing of the present invention
7 facilitates removal of serum and other secretions to
8 minimize the risk of infecting the wound site and macerating
9 the tissue thereat. Growth factor solutions can be
10 important in promoting healing, and antibiotics can be
11 important in preventing and treating infection. Hence, a
12 comprehensive wound treatment can be implemented with the
13 wound dressing and treatment method of the present
14 invention.

15 The wound dressing 10 can be employed to irrigate a
16 wound whereby fluid is introduced and then removed.

17 The operation of the wound dressing 10 is largely a
18 matter of fluid mechanics, and the function of the wound
19 dressing 10 would probably be determined by such factors and
20 variables as: 1) fluid viscosity; 2) permeability of the
21 membrane 22; 3) cross-sectional area of the tube 34 and the
22 area of its opening 39; 4) the integrity of the seal around
23 the membrane perimeter 26; 5) the drawing power of the
24 suction or vacuum source 42; 6) coagulation of the serum or
25 other fluid; 7) the area of the fluid collection chamber 46;
26 8) the length of the tube 34; and 9) gravity and the
27 relative positions of various components. Naturally,
28 varying one or more of these factors or variables could
29 change the operation of the system. It is anticipated that,
30 applying such well-known principles of fluid mechanics, all

17

1 of the wound dressing components could be properly sized and
2 designed. For example, the tube opening 39 could be
3 enlarged, or multiple openings could be provided to increase
4 the rate of fluid flow into the tube 34. The rate of fluid
5 flow can further be increased by locating the tube distal
6 end 38 at a dependent area within the chamber 46, i.e. below
7 the level of most of the wound site 12. The tube 34 can
8 extend downwardly to a collection site below the level of
9 the wound site 12 to facilitate gravity drainage.

10 It is further anticipated that some fluids will resist
11 drainage because of their viscosities or because they tend
12 to coagulate. Drainage of such fluids can be effected by
13 irrigating the wound site 12.

14

15 **IV. First Modified Embodiment 110**

16

17 Figure 8 shows a wound dressing 110 comprising a
18 first modified embodiment of the present invention wherein a
19 relatively small membrane 122 is provided and functions as a
20 patch for a larger wound cover 115 with an opening 117 for
21 receiving a distal end 138 of a tube 134. The primary wound
22 cover 115 is selected to cover a wound site 112, and is
23 placed thereover in the normal fashion. The wound dressing
24 110 can be placed on the primary wound cover 115 in a
25 location chosen to enhance fluid introduction and/or
26 evacuation. For example, to enhance the evacuation of fluid
27 by gravity, it may be desirable to form the opening 117 at a
28 relatively low position of the wound site 112. Thus, fluid
29 will tend to flow to the tube 134 by gravity. To facility
30 the introduction and distribution of fluid, it may be

desirable to locate the wound dressing 110 at a relatively high position on the wound cover 115. In fact, two or more wound dressings 110 could be placed on a single, primary wound cover 115, with a lower wound dressing 110 being provided for fluid evacuation and an upper wound dressing 110 being provided for fluid introduction.

In the practice of the treatment method of the present invention, the wound dressing 110 provides for considerable flexibility in locating the wound dressing 110 in an appropriate location on the wound site 112. After the primary wound cover 115 is positioned, the opening 117 is formed at the chosen location and the wound dressing 110 may be applied, much like a patch, with the tube distal end 138 extending through the primary wound cover opening 117. It will be appreciated that wound dressings 110 may be changed as needed without changing the primary wound cover 115.

V. Second Modified Embodiment 210

A wound dressing 210 comprising a second modified embodiment of the present invention is shown in Figs. 9 and 10 and includes an intermediate layer of material 250 between a wound site 212 and a cover membrane 222. The intermediate material layer 250 can comprise a variety of materials with varying properties such as: 1) absorbency; 2) wicking or capillary action; and 3) surface contact action. The intermediate material layer is primarily located in a chamber 246 formed between the wound 212 and the membrane 222.

1 As a first example of an intermediate material layer
2 250, several hydrophilic colloid materials (i.e.
3 hydrocolloids) are available which would tend to absorb
4 fluids. For example, Envisan wound cleaning pads and paste
5 are available from Marion Laboratories, Inc. of Kansas City,
6 Missouri and comprise: spherical, hydrophilic Beads of
7 Dextranomer, 0.1 to 0.3mm in diameter; polyethylene glycol
8 3000 in the pad; polyethylene glycol 600; and water QS
9 enclosed in a polyamide net bag in the pad or available in a
10 metal foil packet for the paste. The Envisan dextramer
11 beads function to absorb fluid and facilitate healing by
12 drawing fluid from the wound. Excess fluid can be drained
13 from the intermediate material layer 250 to prolong its
14 effectiveness. Other hydrocolloids are commercially
15 available and may be employed with the wound dressing 210 of
16 the present invention, e.g. dextranimers available under the
17 trademark "Debrisan".

18 Alternatively, the intermediate material layer 250 can
19 comprise a mesh or sheet of synthetic material which is
20 generally nonabsorbent and would tend to wick fluid from the
21 wound site 212 to a tube distal end 238. For example, rayon
22 available under the trademark Owens non-adherent surgical
23 dressing from the Davis & Geck Division of American Cyanamid
24 Company of Danbury, Connecticut could be used to form such
25 an intermediate material layer 250, and material available
26 from Marion Merrell Dow, Inc. of Kansas City, Missouri under
27 the trademark "Envinet" could also be employed. Such
28 materials may be referred to as "surface active", i.e.
29 promoting fibrin sealing on the wound surface. Such
30 materials can also satisfy a capillary purpose whereby fluid

1 is wicked from the wound for collection in the chamber 246
2 and ultimately for drainage. With many such materials, a
3 balance is struck between surface action and capillary
4 action, i.e. one such function is often maximized at the
5 expense of the other. For example, Owens rayon is generally
6 considered to be relatively surface active, but may provide
7 less capillary action than other materials. Envinet mesh,
8 on the other hand, provides greater capillary action, but
9 may provide less surface action as compared to the rayon
10 material.

11 Other materials that can be used for the intermediate
12 material layer 250 include polyurethane foam and
13 polyurethane mesh.

14 The wound dressing 210 can be used according to methods
15 for use with the other wound dressings 10 and 110, and
16 includes the additional step of placing the intermediate
17 material layer 250 over the wound site 212. It will be
18 appreciated that there may be a number of materials suitable
19 for the intermediate layer 250 to achieve various
20 objectives.

21 A closure patch 251 is provided for placement over the
22 tube distal end 238 and is adapted for securing it in a
23 folded configuration to the membrane 222. The closure patch
24 251 can be used in conjunction with a bifurcated clip 240 as
25 shown in Figs. 9 and 10, and permits convenient access to
26 the tube distal end 238 for coupling it to various devices
27 such as those described herein, allowing future reuse of the
28 tube or intermittent function. Alternatively, the tube can
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1 be severed at the surface of the membrane, allowing the
2 closure patch 251 or a similar patch of the same material as
3 the wound dressing 10 to permanently seal the tube site.

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5 VI. Third Modified Embodiment 310

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7 A fluidic connection system 310 comprising a third
8 modified embodiment of the present invention is shown in
9 Figs. 11-16. Without limitation on the generality of useful
10 applications of the fluidic connection system 310, it is
11 shown in connection with a urine collection system 312 and
12 functions as a condom catheter. The connection system 310
13 generally includes a membrane assembly 314 and a tube
14 assembly 316.

15 The membrane assembly 314 includes a membrane 318 with
16 an inner or skin contact surface 320, an outer surface 322,
17 a perimeter 324 and an interior portion 326. As shown in
18 Fig. 11, the membrane 318 comprises first and second panels
19 328, 330.

20 The panels 328, 330 include inner contact surfaces 329,
21 outer surfaces 331, perimeters 333, and edges 335 with edge
22 strips 332 which are joined together in opposing relation to
23 form a seam 334 extending transversely across the membrane
24 318 between opposite sides of its perimeter 324. A tube
25 opening 336 extends through the seam 334 approximately in
26 the middle thereof and is open at the membrane inner and
27 outer surfaces 320, 322.

28 An adhesive layer 338 substantially covers the membrane
29 inner surface 320 and releasably secures a two-piece
30 protective backing 340 (e.g. paper, plastic or some other

1 suitable material). The backing 340 can form a transverse
2 seam 342 with a pair of unattached edge strips 344 adapted
3 to be grasped for pulling off the backing 340. The membrane
4 318 of the fluidic connection system 310 can comprise a
5 semi-permeable material.

6 The tube assembly 316 includes an outer tube or sheath
7 346 with proximate and distal ends 348, 350 and a passage
8 347 extending therebetween. The proximate end 348 extends
9 through the tube opening 336 and has a bifurcated
10 configuration with a pair of longitudinally-extending,
11 opposed slits 352 forming an opposed pair of tabs 354 each
12 placed against a respective panel contact surface 320 (Fig.
13 11). The tabs 354 can be secured to the respective panel
14 inner surfaces 320 by the adhesive 338 thereon. However,
15 for many applications of the connecting system 310 it may be
16 preferable for the tabs 354 not to have adhesive on them.
17 The tabs 354 form a mouth 356 open at the outer tube
18 proximate end 348 and located adjacent to the membrane inner
19 surface 320. The outer tube or sheath 346 can comprise a
20 flexible, collapsible, impervious material.

21 The tube assembly 316 also includes an inner tube or
22 conduit 358 with a proximate end 360 including a funnel 362,
23 a distal end 364, and a conduit bore 366 extending between
24 and open at the conduit ends 360 and 364.

25 An annular connector/seal band 372 receives the conduit
26 358 and includes enlarged-diameter end flanges 374 with a
27 reduced-diameter, annular channel or waist 376 therebetween.
28 The connector or seal band 372 can be intergally formed with
29 the conduit and thus permanently fixed in position thereon,
30 or, alternatively, the band 372 can slideably receive the

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1 conduit for adjustable repositioning. Preferably the band
2 372, in either configuration, forms a relatively fluid-tight
3 seal on the conduit 358. The band 372, like the funnel 362,
4 can be slid through the sheath passage 347 for placement
5 proximal to the sheath distal end 350 (Fig. 15). Belt or
6 tie means 378 can be provided for sealingly fastening the
7 sheath 346 to the band 372. As shown in Fig. 15, the
8 belt/tie means 378 can comprise ligatures 380, which can be
9 wrapped around the sheath 346 for tightening it against the
10 band channel 376. Belt/tie means 378 can comprise other
11 suitable fasteners, such as strips with hook-and-loop
12 fasteners (i.e. fasteners available under the trademark
13 "Velcro"), rubber or elastic bands, plastic coated wire
14 twist ties, etc. Multiple bands 372 can be used for
15 connecting and sealing the sheath 346 and the conduit 358.

16 The conduit distal end can project distally from the
17 sheath distal end 350 (Fig. 15) for connection to tubing 382
18 by a suitable tubing connector, such as the multi-diameter,
19 double male-ended ("Christmas Tree") connector 384 shown in
20 Figs. 11 and 15. The tubing 382 can lead to a suitable
21 fluid collection vessel 386, which can be positioned remote
22 from the patient.

23

24 VII. Applications and Operation

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26 The fluidic connector 310 can be utilized for a variety
27 of fluidic connection applications without the inner tube or
28 conduit assembly 358. For example, the fluidic connection
29 system 310 can function as a wound dressing which operates
30 in a manner similar to the wound dressings 10, 110 and 210

1 described above. In such applications the membrane 318 can
2 comprise a semi-permeable, plastic, film adherent dressing
3 sheet, such as those commercially available under the trade
4 names "Op-Site", "Tagaderm", and "Bio-Occlusive". The outer
5 tube or sheath 346 can be utilized as a two-way conduit for
6 draining wound exudate and for introducing liquids to the
7 wound. The liquids introduced could comprise, for example,
8 aqueous solutions for irrigating the wound and growth
9 factors for promoting healing. Epidermal growth factor
10 ("EGF") is available from Vicron. Platelet derived growth
11 factor is available from the Caratech Corporation. Such
12 growth factors can accelerate healing and re-
13 epithelialization of wound sites. Without limitation on a
14 wide variety of wounds that can be treated with such
15 dressings, they are particularly suitable for partial
16 thickness wounds, such as skin graft donor sites. Drainage
17 and liquid application can be alternated without having to
18 intermittently change the membrane 318. Frequent dressing
19 changes can be painful to skin wound patients and burdensome
20 to health care personnel.

21 As with the previously described application of the
22 wound dressing 110 shown in Fig. 8, the connection system
23 310 can be applied at any desired location on a larger patch
24 or membrane, and can be used in various multiple
25 combinations, if desired. For example, one connection
26 system 310 can be used for introducing fluids, and another
27 connection system 310 can be used for draining fluids, with
28 both connection systems 310 operating simultaneously if
29 desired.

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1 To promote efficient drainage, the connection system
2 310 can be located at a dependent part of a larger dressing.
3 Alternatively, mechanical suction equipment can be connected
4 for promoting drainage.

5 Another application of the fluidic connection system
6 310 is placement over percutaneous catheters, drain tubes,
7 etc. Such tubes present infection risks where they
8 penetrate the skin surface, and can require frequent
9 application of antibiotics to reduce the risk of infection.
10 Percutaneous tubes are often sutured in place at the stab
11 wound locations where they penetrate the skin, and the
12 sutures are further susceptible to infection and can cause
13 swelling and patient irritation. The connection system 310
14 can be placed over such a percutaneous drain tube or
15 catheter site, with the tubing extending through the sheath
16 346 in the manner of the conduit 358. The tubing can be
17 secured, for example with one or more bands 372, to protect
18 against traction forces which might otherwise tend to pull
19 the tubing loose. By utilizing a semi-permeable, breathable
20 material for the membrane 318, the skin surrounding a
21 percutaneous tubing entry site can be protected against
22 maceation.

23 For use as a condom catheter in a urine collection
24 system 312, the backing 340 can be removed from the first
25 panel 328, which is then adhesively secured to the ventral
26 side 389 and the lateral sides 391 of a flaccid penis 388
27 with the urethra orifice or meatus 390 directed at the
28 sheath mouth 356 and the sheath tabs 354 placed on the top
29 and bottom of the glans or penile head 392 (Fig. 13). The
30

1 second panel 330, with the backing 340 removed, can then be
2 adhered to the penile dorsal side 394 and to the first
3 panel 328.

4 The procedure described above provides a relatively
5 secure attachment of the connection system 310 to the penis
6 388, since the penile shaft 396 and the penile head 392
7 provide substantial areas of attachment. The attachment can
8 further be enhanced by prestretching the flaccid penis to
9 provide maximum contact area.

10 The connection system 310 described above can be
11 utilized as a complete condom catheter by fluidically
12 connecting the sheath distal end 350 to a suitable urine
13 vessel, for example with a band such as that shown at 45 in
14 Fig. 7. Alternatively, the inner tube or conduit 358 can
15 then be inserted through the sheath passage 347 in its open,
16 distal end 350. The funnel 362 can be placed against the
17 glans 392 over the meatus 390, and can be secured in this
18 position by fastening the sheath 346 to the band 372 with
19 the sheath 346 slightly in tension and the conduit 358
20 slightly in compression. The funnel 362 can comprise a
21 moldable plastic material, and its end can be rolled or
22 flanged as shown in Fig. 14 for patient comfort. However,
23 in operation the funnel 362 is not required to form a fluid-
24 tight seal with the glans 392, and it is anticipated that
25 the funnel 362 may slip distally away from the glans 392.
26 The funnel 362 cooperates with the connection system 310 to
27 direct a surge of urine into the conduit 358. Urine which
28 escapes the funnel 362 can collect in an interstitial space
29 397 between the sheath 346, the conduit 358, the glans 392
30 and the band 372. Urine in the interstitial space 397 can

1 drain to the funnel 362 for evacuation through the conduit
2 358. Placement and sizing of the sheath 346, the conduit
3 358 and the band 372 can be adjusted to vary the volume of
4 the interstitial space 397.

5 The procedure for applying the connection system 310
6 can be varied according to the conditions of particular
7 patients and the preferences of persons applying it.
8 Properly adhered to a patient, the collection system 310
9 should be functional for a relatively long period of time,
10 and a semi-permeable membrane material can be utilized to
11 enhance patient comfort.

12 Other useful applications of the connection system 310
13 include placement over circumferentially injured limbs and
14 phalanges for draining exudates and/or introducing liquids.
15 For example, an injured hand could be treated by securing
16 the connection system 310 at the wrist, a forearm could be
17 treated by adhering the fluidic connection system 310 at
18 the elbow, etc.

19 Yet another application is for accessory connections
20 whereby various fluid devices and connectors could be
21 combined in systems attached to patients for appropriate
22 treatment and diagnostic procedures. Such additional
23 accessories include Jackson-Pratt and Blake suction tubing
24 devices, Y-connectors, sampling ports, "Injectaport"
25 devices, fluid pumps and various fluid reservoirs. Hand-
26 actuated bulbs could be placed in the tubing, and valving
27 could be placed where it is needed.

28 A further application of the fluidic connection system
29 310 would involve placing the membrane 318 over an
30 intermediate material layer 250 as described in connection

1 with the wound dressing 210 comprising a second modified
2 embodiment of the present invention (Figs. 9 and 10). An
3 inner tube or conduit such as that shown at 358 could then
4 be extended through the sheath 346, secured thereto by a
5 band or bands 372, and the inner tube or conduit distal end
6 364 could be placed beneath the intermediate material layer
7 250 adjacent to the tissue surface at the wound site 212, or
8 the conduit distal end 364 could be embedded within the
9 intermediate material layer 250. The inner tube or conduit
10 358 could then be used for draining exudate from or
11 introducing fluids to the wound 212.

12 It is to be understood that while certain forms of the
13 present invention have been illustrated and described
14 herein, it is not to be limited to the specific forms or
15 arrangement of parts described and shown.

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CLAIMS:

1. A fluidic connection system, which comprises:
- (a) covering means with a skin contact surface and an outer surface;
- 5 (b) adhesion means on said skin contact surface for releasably coupling said covering means with a skin surface;
- (c) said covering means including first and second panels connected to each other along a seam extending transversely across said covering means;
- 10 (d) said seam forming an opening between said first and second panels for receiving a tube; and
- (e) tube means having a proximate end extending through said opening and terminating adjacent to said skin contact surface for fluidically communicating with said skin
- 15 contact surface.
2. The fluidic connection system of claim 1 wherein said covering means comprises a semipermeable material.
3. The fluidic connection system of claim 1 wherein said adhesion means comprises an adhesive coating on said contact
- 20 surface.
4. The fluidic connection system of claim 1 wherein said tube means comprises a flexible, collapsible material.
5. A fluidic connection system, which comprises:
- (a) covering means with a skin contact surface and
- 25 an outer surface;

(b) adhesion means on said skin contact surface for releasably coupling said covering means with a skin surface;

(c) said covering means having an interior portion including an opening extending between and open at said skin
5 contact and outer surfaces thereof;

(d) tube means having a proximate end extending through said opening and terminating adjacent to said skin contact surface and a distal end located outwardly from said outer surface, said tube means fluidically communicating with
10 said skin contact surface;

(e) said tube means proximate end including an opposed pair of longitudinally-extending slits; and

(f) a pair of opposed end tabs are each formed between said slits, said tube means proximate end being open
15 between said tabs.

6. The fluidic connection system of claim 5 wherein:

(a) each said tab is adhesively connected to said contact surface.

7. A fluidic connection system, which comprises:

20 (a) covering means with a contact surface and an outer surface, said covering means including:

first and second panels each having a perimeter and an edge;

each said panel having an inner contact surface
25 and an outer surface;

a seam extending transversely across said covering means and extending outwardly from said outer surfaces of said panels, said seam formed by connecting said panels at their respective contact surfaces adjacent to their respective edges and said seam having opposed ends; and

an opening extending through said seam between said inner surfaces of said panels and intermediate said opposed ends, said opening extending between and opening at adjacent edges of said panels and at said inner surface;

(b) adhesion means on said contact surface for releasably attaching said covering means;

(c) said covering means having an interior portion with an opening extending between and open at the contact and outer surfaces thereof; and

(d) tube means having a proximate end extending through said opening and terminating adjacent said contact surface and a distal end located outwardly from said outer surface, said tube means fluidically communicating with said contact surface.

8. The fluidic connection system of claim 7 wherein said covering means comprises a semi-permeable material.

9. The fluidic connection system of claim 7 wherein said tube means includes:

(a) an outer, tubular sheath connected to said panels at said seam and having a proximate end, a distal end, and a sheath passage extending between said sheath proximate and distal ends; and

(b) an inner, tubular conduit extending through said sheath passage and including conduit proximate and distal ends and a conduit bore extending between said conduit ends.

10. A fluidic connection system which comprises:

5 (a) covering means with a contact surface and an outer surface;

(b) adhesion means on said contact surface for releasably attaching said covering means;

(c) said covering means having an interior portion
15 with an opening extending between and open at the contact and outer surfaces thereof; and

(d) tube means having a proximate end extending through said opening and terminating adjacent said contact surface and a distal end located outwardly from said outer
15 surface, said tube means fluidically communicating with said contact surface, said tube means including:

an opposed pair of longitudinally-extending slits; and

a pair of opposed end tabs each formed between
20 said slits, said tube means proximate end being open between said tabs.

11. A fluidic connection system, which comprises:

(a) covering means with a contact surface and an outer surface;

25 (b) adhesion means for releasably coupling said covering means with said contact surface;

(c) said covering means having an interior portion with an opening extending between and open at the contact and outer surfaces thereof;

(d) tube means having a proximate end extending
5 through said opening and terminating adjacent said contact surface and a distal end located outwardly from said outer surface, said tube means fluidically communicating with said contact surface;

(e) said covering means including first and second
10 panels interconnected at a seam; and

(f) said tube means including:

an outer, tubular sheath connected to said
panels at said seam and having a proximate end, a distal end,
and a sheath passage extending between said sheath proximate
15 and distal ends; and

an inner, tubular conduit extending through said
sheath passage and including conduit proximate and distal ends
and a conduit bore extending between said conduit ends.

12. The fluidic connection system of claim 11 wherein:

20 (a) said conduit includes funnel means at its proximate end, said funnel means being adapted to slide longitudinally through said sheath passage.

13. The fluidic connection system of claim 11 wherein
said tube means includes:

25 (a) tube clamp means clamping said sheath to said inner conduit.

14. The fluidic connection system of claim 13 wherein said tube clamp means comprises:

(a) an annular band with enlarged proximate and distal ends, a bore extending between said ends and a reduced-diameter waist between said ends, said bore receiving said conduit; and

(b) belt means circling said sheath and securing said sheath to said band waist.

15. The fluidic connection system of claim 14 wherein:

(a) said belt means comprises a tensile member wrapped around said sheath and said band waist.

16. The fluidic connection system of claim 14 wherein:

(a) said belt means comprises a strap with hook-and-loop fasteners.

15 17. A fluidic connection system which comprises:

(a) covering means including:

an inner contact surface;

an outer surface;

a first panel including a perimeter and an edge;

20 a second panel including a perimeter and an edge;

each said panel having an inner contact surface and an outer surface;

a seam extending transversely across said covering means and comprising said panels being coupled together at their respective edges, said seam having opposed ends; and

5 an opening extending through said seam between said panel contact surfaces and intermediate said seam ends, said tube opening extending between and open at said adjacent panel edges and at said contact surfaces;

(b) an adhesive coating on said panel contact
10 surfaces; and

(c) tube means including a proximate end extending through said opening and terminating adjacent said skin contact surface, said proximate end having an opposed pair of longitudinally-extending slits and a pair of opposed end tabs
15 each formed between said slits, said tube means proximate end being open between said tabs.

18. The fluidic connection system of claim 17 wherein said tube means includes:

(a) an outer, tubular sheath connected to said
20 panels at said seam and having approximate end, a distal end, and a passage extending between said sheath proximate and distal ends; and

(b) an inner, tubular conduit extending through said sheath passage and including conduit proximate and distal ends
25 and a conduit bore extending between said conduit ends.

19. The fluidic connection system of claim 18 wherein:

(a) said conduit includes funnel means at its proximate end, said funnel means being adapted to slide longitudinally through said sheath passage.

5 20. The fluidic connection system of claim 18 wherein said tube means includes:

(a) tube clamp means clamping said sheath to said inner conduit.

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